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DEVICE FOR CONTROLLING EXTRA-VASCULAR HAEMORRHAGE

The present invention relates to devices for controlling extra
5 vascular haemorrhage and, in particular, to an inflatable
device for use as an intravascular haemostatic device.

Damage of injury to blood vessels may lead to extravasation
(bleeding out from blood vessels). Such internal bleeding
10 leads, in turn, to loss of blood-pressure in the patient
having the damaged or injured blood vessel. Extravasation is
particularly dangerous to the patient where the damaged
vessels are the retro-hepatic vena cava and/or the hepatic
veins as these blood vessels are very difficult to reach by a
15 surgeon for repair thereof. These blood vessels are located
close to the spine and behind the liver, and for a surgeon to
repair a damaged vessel of this type it is first necessary for
the surgeon to be able to have relatively unhindered access to
the vessel. Usually, access to damaged blood vessels may be
20 achieved by relatively straightforward dissection. However,
in the case of damage to the retro-hepatic vena cava or the
hepatic veins the emergency dissection required is
particularly difficult as the surgeon must generally dissect
anteriorly with the bulk of the liver directly in the way with
25 the result that access is obstructed. This is a very time
consuming procedure and furthermore is not a procedure
encountered on a regular basis by the majority of surgeons due
to the relatively infrequent occurrence of damage to these
vessels (retro-hepatic vena cava and hepatic veins).

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A further complication in these types of procedures is that
further blood loss may result from the surgery procedure
itself (iatrogenic damage). This complication may also be
further aggravated, in part, by the surgeon performing such an
35 unfamiliar procedure.

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Procedures to repair damaged blood vessels must in general be performed as quickly as possible to minimise the degree of extravasation. Control of extravasation must be achieved at
5 the earliest opportunity i.e. within a matter of a few minutes at most, especially where a major blood vessel is damaged. It is possible for total exsanguination to occur within two or three minutes. Injury or damage to the liver itself, particularly where there is severe disruption to the liver
10 architecture by penetrating injury, avulsion of the liver, or maceration of the liver itself resulting in loss of integrity of the liver's own blood vessels, and thus haemorrhage, is associated with high mortality and morbidity. Difficulty in achieving timely control of extravasation results generally in
15 blood flowing back along the hepatic veins and out through the damaged/injured liver and into the peritoneum. The difficulty in controlling extravasation is inter alia a direct result of the difficulty of the surgeon gaining quick access to the injury site and then establishing control of the
20 extravasation. It is also difficult to both operate and control haemorrhage at the same time.

Once a surgeon has gained access to the injured or damaged vessel or organ, in order to repair the damaged portion
25 thereof, it is necessary to at least temporarily control the extravasation from the injury or damaged portion of the vessel or organ. This at least temporary control of extravasation allows the surgeon to effect a repair to the injured/damaged vessel or organ. In techniques where such temporary control
30 is imposed, the organs or other body part(s) supplied by blood from the damaged vessel (or for blood returning to the heart) may be starved of blood (ischaemia). This can have serious consequences such as organ damage, or mortality. Temporary control of extravasation from the damaged/injured vessel/organ
35 must therefore not substantially prevent blood flow to or from

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an organ or body to be supplied therefrom, if these serious complications are to be avoided.

Previously, temporary control of extravasation has been
5 attempted using shunting techniques. "Insertion of a
Retrohepatic Vena Cava Balloon Shunt Through the
Saphenofemoral Junction" (OJ McAnena, EE Moore & FA Moore),
The American Journal of Surgery, Vol.158, November 1989
described a retrohepatic vena cava balloon shunt. The device
10 is relatively big and clumsy, and relies on the use of an
intercostal chest drain, normally used for draining air,
blood, pus or other fluid out of the chest, and an inflatable
balloon to occlude the damaged portion of the vessel. This
device also requires time-consuming dissection of the patient
15 and relatively complex surgical manoeuvres in order to insert
and use the device. Only surgeons and theatre staff practised
in the technique of insertion which is required would be able
to use the device competently. Moreover, blood flowing in the
damaged vessel must ingress into the shunting tube through
20 small holes provided in a section of the tube close to the
balloon, and exit from more small holes in the shunting tube
after the balloon, in order to bypass the balloon. This
results in restriction of blood flow in the vessel which is a
major disadvantage. Particularly in shocked patients where
25 blood circulating volume needs to be restored as soon as
possible, any restriction of flow will have a deleterious
effect and may be primarily responsible for the death of the
patient.

30 It is an object of the present invention to avoid or minimise
one or more of the abovementioned problems.

According to a first aspect of the invention, there is
provided an inflatable device for inserting, in a
35 substantially deflated state, into a blood or other biological

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fluid carrying vessel of a human or animal, the device having an inflated state in which it defines elongate open-ended tube means via which the blood or other biological fluid in the vessel flows through the device in use thereof.

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More specifically, but not exclusively, the invention provides an inflatable device for inserting, in a substantially deflated state, into a damaged blood or other biological fluid carrying vessel of a human or animal, and
10 having an inflated state for substantially occluding the damaged portion of the vessel so as to minimise, preferably substantially prevent, leakage from said damaged portion, wherein the device in its inflated state defines elongate open-ended tube means via which the blood or other biological
15 fluid in the vessel flows through the device in use thereof, whereby said damaged portion of the vessel is bypassed.

One advantage of the invention is that the device can be located within the blood/biological fluid conveying vessel at
20 the site of the damaged portion thereof, and then inflated to its inflated condition so as to occlude the damaged portion of the blood/biological fluid conveying vessel, thereby preventing extravasation therefrom while at the same time allowing blood/biological fluid to flow relatively
25 unrestricted through the device. In this manner normal, or near normal, anatomical and physiological blood flow in the vessel can be maintained. This is particularly important for shocked patients, where blood has extravasated or come out of the vessels and been lost to the circulation. Moreover, the
30 tubular form of the device also facilitates the occlusion of cuts, tears or other apertures in the vessel of various sizes and shapes. The device of the present invention may also be used instead of techniques such as atriocaval shunting where access to the patient's heart is required for insertion of,
35 for example, a chest tube/drain into the pericardial cavity.

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Using conventional equipment, such shunting requires a large degree of dissection to provide access to the heart. The device of the present invention reduces the degree of dissection necessary for insertion of a chest tube compared to 5 that required for inserting the device into the Inferior Vena Cava (IVC) below the hepatic veins and moving one end of the device inside the IVC and into the pericardium.

The elongate tube means defined by the inflated device is 10 preferably substantially cylindrical in form, having an inlet end and an outlet end and passage means, comprising at least one passage, defined therebetween, through the longitudinal length of the device. The cylindrical form provides a close fit with the lumen of the damaged vessel. The diameter of 15 said passage means is preferably sufficiently large that the blood (or other biological fluid) may flow relatively unhindered through the device. Thus, the diameter of said passage means may be at least 50%, preferably greater than 50%, most preferably in the range of 90 to 95%, of the outer 20 diameter of the inflated device.

The device of the present invention operates in the manner of an inflatable sleeve which may be inserted intra-vascularly and located at an injury site e.g. a rupture in a blood 25 vessel, from which blood is escaping. The size of the inflated device is chosen such that upon inflation of the device, an outer wall of the device presses against the intima of the blood vessel at the rupture, forming a seal which prevents blood from escaping from the rupture in the vessel 30 while at the same time the tubular form of the inflated device allows blood to continue to flow relatively unhindered through the device, following its natural flow path in the vessel.

The inflatable device preferably comprises one or more 35 substantially collapsible walls defining a substantially

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enclosed inflatable volume. For example, the device may conveniently comprise a balloon shaped so as to define said elongate tube means when inflated. The device can be inflated by injecting saline or another physiologically acceptable fluid, or combination of fluids, into the enclosed inflatable volume.

The device may be generally circular in cross-section. Alternatively, it may be formed with an elliptical or irregular cross-section, according to the particular shape or configuration of the damaged blood or biological fluid carrying vessel in which the device is to be used.

It will be generally appreciated that the relative length and diameter dimensions of the device may be varied (at manufacture) according to the particular requirements of the use to which the device may be put. For example, where the device is to be deployed within a relatively large internal diameter vessel such as the inferior vena cava (IVC) or aorta, it would be necessary to use a device with correspondingly large diameter; conversely where the device is to be used in a relatively small internal diameter vessel such as femoral or subclavian arteries, a correspondingly small diameter is required.

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The longitudinal length of the inflatable device may be varied similarly (at manufacture) according to need. For example, where the area of injury is quite extensive along the length of the blood vessel, then it would generally be necessary to use a device of a length sufficient to extend to at least the same length as the injury area of the vessel (and preferably slightly greater length).

The device of the present invention is preferably provided with a working channel (or conduit) which may conveniently be

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substantially aligned with a longitudinal axis of the device. More preferably, the working channel or conduit is formed and arranged to extend at least part-way through the longitudinal extent of the device. Desirably, the working channel or
5 conduit formed and arranged for receiving therein at least one of : fluids, devices and a guide-wire. It will of course be appreciated that where the working channel/conduit can be utilised to locate or deliver said fluids, devices or guide wire to a location within the device (such as the passage
10 means) or to a location exterior to the device depending upon *inter alia* the longitudinal extent of the working channel/conduit. Where, for example, the working channel/conduit is intended to be used for receiving a said guide-wire or device, it will be appreciated that the working
15 channel need not be a totally enclosed channel (such as a pipe), but may be a channel being of a C-shaped cross-section which would be sufficient to retain the guide-wire or device therein, but would not be suitable to receive a fluid therethrough. According to one embodiment of the invention,
20 the working channel is the hollow interior of a central elongate conduit or similar such structure which may be integrally formed with the inflatable device, or may be fixed to the device at at least one point therealong, with opposite end portions of the elongate conduit protruding from
25 respective opposite ends of the tube means defined by the inflated device. A first one of said protruding end portions is preferably relatively long, for example up to approximately one metre long, while the second end portion protrudes only a very short length beyond the tubular form of the inflated
30 device (e.g. only a few centimetres). Said first protruding end portion is preferably provided with a first self-sealing entry port to allow the admission of fluids, such as saline or image contrast materials, or other materials or devices, into the working channel, for delivering into the patient's
35 bloodstream.

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A further advantage of the working channel is that it enables a said guide wire to be inserted therealong to assist in the insertion and positioning of the device in the patient. Thus, 5 a further significant advantage is that the device does not require unusual insertion techniques. It can be inserted relatively straightforwardly by a surgeon or an anaesthetist. For example, where the device is to be used for temporary control of extravasation from the retro-hepatic vena cava, or 10 the hepatic veins, a surgeon or anaesthetist can insert the device quickly from above by inserting it into a major vein in the patient's neck (the lumen of the Internal Jugular Vein is in direct continuity with that of the IVC via the Right Atrium of the heart). Also, the device is not orientation dependant 15 i.e. it cannot be inserted "upside down", since it is basically an inflatable tube.

A wall of the elongate conduit preferably contains, in the thickness thereof, a second channel which is in fluid 20 communication with the inflatable volume of the device, and via which saline or other biologically compatible fluid is injected into the device in order to inflate the device. In this case an input end (for receiving the saline) of the second channel preferably terminates in and is connected to a 25 second self-sealing entry port provided in the same end portion of the elongate conduit as the first entry port. In use, saline is injected via said second self-sealing entry port, along the second channel in the elongate conduit, to inflate the device. The wall(s) of the central elongate 30 conduit may contain one or more further channels in fluid communication with further separate entry ports provided on the same protruding end of the central elongate conduit, for separately carrying saline, contrast imaging fluids or other fluids or devices (e.g. blood or fluid for resuscitation 35 purposes) therealong, to, from or through the device.

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The device may be fabricated from one or more physiologically acceptable materials such as various rubber, synthetic rubber, or plastics materials e.g. latex, polyvinyl chloride, polyurethane, polyethylene, Pluronic (RTM), and/or block, and/or co-polymers thereof. For example, the inflatable tube means may be made of latex while the central elongate conduit may conveniently be made of polyurethane.

10 The device may further include at least one inflatable support strut within the passage means of the device and which may span the inner diameter of the device. The or each said support strut preferably has a hollow interior which is in fluid communication with the enclosed inflatable volume of the device. The or each said support strut provides additional structural integrity to the device when deployed to its at least partially or fully inflated condition. Various configurations of said support strut are possible. Moreover, a plurality of support struts may be provided e.g. two, three, 20 four or more support struts. These support struts are preferably formed and arranged such that, in the inflated state of the device, the struts extend radially outwardly from the central elongate conduit to an annular outer portion of the preferably generally cylindrical form of the inflated 25 device.

The support struts are, in the preferred embodiment, fluidly connected to the inner, saline carrying, channel formed in the wall of the central elongate conduit as above-described, whereby the device is inflated by injecting saline (or another physiologically compatible fluid) through this inner channel in order to inflate the support strut and, consequently, the annular outer portion of the device.

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In a further preferred embodiment of the device, the tube forming the device is formed from at least two inflatable semi-circular wall portions, each wall portion having two major longitudinally extending edges which extend
5 substantially parallel to a corresponding edge of an adjacent wall portion; said at least two wall portions is in fluid communication with a support strut, wherein said support strut is formed and arranged to align the respective major edges of the at least two wall portions such that the major edges of
10 adjacent wall portions abut against one another to form a more or less fluid tight seal therebetween and along the extent thereof when the device is in an inflated condition.

Preferably, more than one strut is provided per wall portion.
15 Two, three or four struts can be provided per wall portion.
Desirably two struts are provided per wall portion.

It will of course be appreciated that where the tube comprises only two wall portions, then only a single strut which extends
20 between the two wall portions need be provided to ensure that the major edges of adjacent wall portion are maintained in alignment with one another.

Where three, four, five or more wall portions are provided,
25 then each wall portion is provided with a strut, wherein each strut is adjoined to a strut of an adjacent wall portion. In such an arrangement the wall portions may be individually and separately inflatable via said struts, or may be inflated together when said struts are all in common fluid
30 communication with one another.

The inflated device may be non-uniform in outer diameter along the longitudinal length thereof. The required device preferably comprises end portions and a waist portion disposed
35 therebetween, wherein the waist portion has a reduced outer

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diameter portion extending at least part-way around the circumference of the waist portion, whereby when inflated within a blood/biological fluid conveying vessel, the end and waist portions provide a leak-proof fit between the inner wall 5 (intima) of the vessel and the outer surface of the device, and the reduced diameter portion defines a working cavity between the outer surface of the device and the intima.

Desirably, the reduced outer diameter portion extends 10 longitudinally of the length of inflated device to at least the same extent as the extent to which the reduced outer diameter portion extends around the circumference of the inflated device i.e. the inflated device resembles a "canoe" type shape. Most preferably, the inflated device presents a 15 generally hour-glass shaped side profile, having a relatively narrow waist portion and relatively wide end portions. In this embodiment the wide end portions, when the vessel is in its inflated condition, provide a leak-proof fit with the inner wall (intima) of the blood/biological fluid conveying 20 vessel. The relatively narrow waist portion defines a working space between the outer surface of the device and the damaged portion of the blood/biological fluid conveying vessel, in which working space a surgeon can effect repair to the damaged area.

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Furthermore, the hour-glass shaped device may be of particular use within branched vessels such as the Inferior Vena Cava (IVC) which has attached blood vessels such as the hepatic veins. For example, during a liver transplant the hour-glass 30 shaped device may be inserted into the IVC (in a deflated condition) so that one end of the device is positioned above the hepatic veins and the other end is positioned below the hepatic veins. Inflating the device provides a leak tight fit between the ends of the device and the intima of the IVC while 35 maintaining blood-flow through the IVC, and at the same time

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isolating the hepatic veins from the blood flowing through the IVC. A "cuff" of the hepatic veins may be formed by incising around the hepatic veins at the point of attachment to the IVC thereby allowing removal of the liver and the hepatic veins
5 while maintaining blood-flow through the IVC.

In a modified embodiment, the device incorporates a waist portion which is separately inflatable to the rest of the inflatable volume of the device. By at least partially
10 deflating the separately inflatable waist portion, when the device is in situ, a generally annular working space between the waist portion and the wall of the damaged vessel can be created and/or enlarged.

15 In a further embodiment of the above-described invention, the device is provided with one or more strategically positioned openings formed and arranged to allow perfusion of blood therethrough from the passage means defined in the inflated device, in a flow direction generally perpendicular to the
20 axis of the device, to branching blood vessels whose inlet ends are located adjacent the openings in the device, when the device is correctly positioned in use thereof. Additionally, for example, the device may be inserted into a vein whereby blood would be permitted to flow from an associated organ, eg
25 a kidney or liver, thus maintaining perfusion while isolating a damaged portion of the vein which can be repaired. The device may have a non-uniform diameter along its length, having a relatively narrow first end portion (neck portion) being provided with said openings, and a relatively wide
30 second portion (body portion).

According to yet another aspect of the invention there is provided a kit of parts comprising an inflatable device as described above, for inserting into a damaged blood or other
35 fluid carrying vessel, and insertion means for facilitating

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access to the inside of said vessel. The kit-of-parts preferably also includes deployment means for deploying the balloon to its inflated condition.

- 5 The insertion means may conveniently comprise a needle for gaining access to a portion of the blood vessel (or other biological fluid carrying which is damaged (or other blood vessel connected vessel) thereto), and a guide wire for inserting into the blood vessel through a bore of the needle.
- 10 The insertion means preferably further includes sheath means through which the inflatable device may be inserted into the blood vessel. The elongate guide wire is preferably flexible when transverse force is applied to it to allow it to flex or bend without being permanently deformed. The sheath is
- 15 preferably tubular in form, and is advantageously tapered at one end thereof to facilitate insertion into the lumen of the damaged blood vessel.

The inflatable device is preferably provided with a central

20 elongate conduit, as above described, having a working channel through which the guide wire may be inserted, and a second channel which is in fluid communication with the inflatable volume of the device. The deployment means preferably comprises syringe means for injecting saline, or another

25 biologically compatible fluid, into the inflatable device via said second channel in the elongate conduit.

By means of the above-described kit, the inflatable device can be inserted and deployed in the abdomen of a patient by a

30 surgeon, or alternatively and more conveniently by another doctor outside the operative field (e.g. an anaesthetist).

According to another aspect of the invention use of an inflatable device as above-described, in therapy, is claimed.

35 In particular, use of the above-described inflatable device in

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the control of extra-vascular haemorrhage is claimed, and especially use of the above-described inflatable device in occluding a damaged portion of the inferior vena cava, or one of the hepatic veins.

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According to a further aspect of the invention there is provided a method of controlling extra-vascular haemorrhage comprising inserting the above-described inflatable device, in its deflated condition, into a damaged blood vessel, locating
10 the device adjacent to a damaged portion of the blood vessel, and inflating the device so as to substantially occlude the damaged portion so as to minimise, preferably substantially prevent, leakage of blood from said damaged portion. The damaged blood vessel may, for example, be the inferior vena
15 cava, or one of the hepatic veins. In this case, the insertion step of the method preferably comprises inserting the device in a vein in the neck of the patient.

Alternatively the vessel may be the aorta and the damaged
20 portion thereto may, for example, be a tear in the aorta resulting from traumatic disruption of the aorta or injury to the arch of the aorta. In this case, access via the arterial system is necessary and thus the insertion step may conveniently comprise inserting the device into the patient
25 from below, via the femoral artery.

Further applications of the above-described inflatable device are also possible. In particular, the device may find application in the field of stenting. In conventional stenting
30 blood flow is temporarily blocked when the balloon carrying the (collapsed) stent is inflated. It is well known that inserting a stent into a vessel, such as the Thoracic Aorta, has a particular problem associated therewith in that both the balloon and the stent migrate in the direction of the blood-
35 flow through the vessel as the balloon is inflated. The

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migration is a result of the balloon acting effectively as a piston within the vessel whereby the blood acts directly thereagainst. This problem of stent and balloon migration is undesirable, especially where each stent is relatively
5 expensive and in some cases are custom-made for a particular patient and surgical procedure. In contrast, the tubular form of the inflated device of the present invention will allow blood to flow relatively unrestricted therethrough during expansion of the stent. Thus, in accordance with another
10 aspect of the invention there is provided a method of inserting and deploying a stent in a blood vessel, the method comprising the steps of: locating an expandable generally tubular stent, in a collapsed state thereof, on the above-described inflatable device so that the stent is coaxial with
15 and circumferentially surrounds the inflatable device; inserting the inflatable device, in its deflated condition, and with the stent located thereon, into the blood vessel to be stented and locating the device in the desired portion thereof; and inflating the device so as to deploy the stent to
20 an expanded condition in which it supports the wall of the blood vessel.

Preferred embodiments of the invention will now be described by way of example only and with reference to the accompanying
25 drawings in which:

Fig. 1 is a plan view of a device according to one embodiment of the invention, being inserted into a blood vessel;

Fig. 2 is a side view of the device being inserted into the blood vessel as in Fig. 1, the blood vessel being shown in
30 cross-section so as to reveal the portion of the device inserted therein;

Fig. 3 shows the device of Figs. 1 and 2, deployed (i.e. in its inflated state) in the blood vessel which is again shown in cross-section;

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Fig. 4 is an end cross-section of the inflated device of Fig. 3;

Fig. 5 is a longitudinal sectional view of an inflated device according to another embodiment of the invention, shown

5 located in a blood vessel;

Fig. 6 is a longitudinal sectional view of an inflated device according to a further embodiment of the invention;

Fig. 7 is a side view of a device according to a yet further embodiment of the invention, having a reduced diameter end

10 portion with openings therein;

Fig. 8 illustrates blood-flow pathways through the device of Fig. 7;

Fig. 9 shows the device of Figs. 7 and 8, in an inflated condition, in situ in a blood vessel with a leaking aneurysm, 15 the blood vessel being shown in cross-section so as to reveal the device;

Fig. 10 is a side view of an inflated device according to a yet further embodiment of the present invention;

Fig. 11 is a plan view looking down onto the device of Fig. 20 10;

Fig. 12 is a schematic side view of the device of Figs 10 and 11 located within the Inferior Vena Cava adjacent the hepatic veins and liver;

Fig. 13 shows the liver of Fig. 12 with a cuff cut from the 25 Inferior Vena Cava;

Fig. 14A and Fig. 14B shows a section of a further preferred embodiment of the device in deflated and inflated conditions respectively where the tube is formed from three separate wall portions adjoined by struts.

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An inflatable device 1 according to one embodiment of the present invention is shown in Figs. 1-4. Figs. 1 and 2 show the device in its deflated condition being inserted, via a sheath 2 provided for use with the device 1, into a blood 35 vessel 4 which has a damaged portion 6. The device 1 comprises

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a balloon which, when inflated (as shown in Fig. 3), defines a generally tubular member of substantially cylindrical open-ended form, a passage 8 being defined therethrough by an inner wall 10 of the device 1, as shown most clearly in Fig 4.

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As illustrated in Figs. 1 & 2, to facilitate insertion of the device 1 into a blood vessel 4 a sheath 2 is provided for insertion into the blood vessel 4. In Figs. 1-3 the sheath 2 is shown as transparent in order to reveal the device 1 being pushed therethrough into the lumen of the blood vessel. A first, slightly tapered, end 14 of the sheath 2 is inserted into the blood vessel 4 and a second end of the sheath 2 protrudes from the blood vessel 4. The second end 16 of the sheath 2 is self-sealing around a central elongate tube 20 which extends through, and protrudes rearwardly from, the inflatable device 1. The insertion procedure is described in further detail herebelow.

As seen most clearly from Figs. 3 & 4, the central tube 20 extends axially through the passage 8 and protrudes from each end of the device. The central tube 20 is hollow, the hollow interior acting as a working channel 23 for delivery of fluids into the damaged blood vessel, beyond the damaged portion 6 thereof. A smaller separate channel 21 which is in fluid communication with the inflatable volume of the device 1, is incorporated within the thickness of the wall 25 of the central tube 20. Three elongate inflatable struts 22 branch outwardly from the working channel 23 to the inner wall 10 of the device 1, effectively dividing the passage 8 into three separate passage sections 8a, 8b, 8c, and are in fluid communication with the central tube 20 which is provided at a first end 20a thereof with a self-sealing side entry port 24 for the injection of saline (or other physiologically compatible fluid) into this smaller channel 21 to effect inflation of the device 1. A second self-sealing side entry

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port 26 is also provided at the first end 20a of the central tube 20 for injection of contrast fluids or other materials into the blood vessel 4, via the working channel 23, for imaging or other similar purposes. The first and second entry ports 24, 26 are connected to one end of the smaller channel 21 and working channel 23 respectively. As shown in Figs. 2 and 3 there is a relatively long length (approx. one metre or so) of central tube 20 between the inflatable portion of the device and the first end 20a of the central tube having the side entry ports 24, 26. The other end 20b of the central tube protrudes only a short way (a few centimetres) beyond the inflatable tube portion of the device.

A guide wire (not shown) is used to facilitate insertion and positioning of the device 1 in the blood vessel 4. The guide wire is formed from a physiologically compatible alloy of metal such as known medical quality steels (stainless steels). In use, the device 1 is inserted as follows. Firstly, a small incision is made in the patient's skin in the region of, but not into, a blood vessel (e.g. vein or artery) into which the device 1 is to be inserted. This blood vessel could be the vessel having the damaged portion, or a vessel connected to the damaged one and through which access to the damaged vessel can therefore be obtained. For example, when the damaged vein is the inferior vena cava, access thereto can be obtained by inserting the device 1 into the internal jugular vein in the patient's neck, connected to the superior vena cava. A needle (hypodermic) is then used to locate the blood vessel itself, by inserting the needle thereinto (via the incision in the skin). A guide wire (not shown) is then threaded through the needle, into the blood vessel. The needle is then removed. A dilator (not shown) can then be used to enlarge the opening into the blood vessel (created by the needle) and, after removing the dilator, the tapered end 14 of the sheath 2 is inserted into the aperture. The working channel of the

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elongate tube member is then threaded over the guide wire and the device 1 is pushed (manually) therealong, through the sheath 2. The guide wire can be removed at this point (and in any case is removed prior to inflation of the device 1). The device 1 is continued to be pushed along the lumen of the blood vessel, through the sheath 2, with the long end of the central tube 20 trailing behind the deflated device 1, until the device 1 is located adjacent to the damaged portion 6 in the wall of the blood vessel. The device 1 is then inflated by the injection of saline, so as to occlude the damaged portion 6.

The device 1 in an inflated condition, as shown in Fig. 3, comprises a generally cylindrical member which is supported at least in part by the inflatable support struts 22. As afore-described, the support struts 22 are in fluid communication with the inflatable volume of the device 1 and receive saline solution (or another physiologically acceptable fluid which is injected into the inflatable volume of the device) from the inflation channel 21 in the central tube 20. When inflated, the outer wall 28 of the device 1 is pressed flush against the inner wall (intima) 30 of the blood vessel 4, to form a leak-free seal between the device 1 and the inner wall of the vessel 4. With the device in its inflated condition, as shown in Figs. 3 and 4, blood flows through the passage 8 (see arrows A to B, Figs. 5, 6) relatively unhindered, while the damaged portion 4 of the vessel 2 is repaired by a surgeon. (Blood may alternatively flow in the direction of B to A in Figs. 5 and 6). The diameter of the passage 8 is sufficiently large to ensure that blood flows through the device 1 relatively unhindered i.e. at or approaching normal flow rates in the vessel. This is achieved by designing the diameter of the passage means to be in the range of 80 to 90% of the outer diameter D of the device.

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Preferably, at least those surfaces of the device which will be in contact with blood are formed from and/or coated with an anticoagulant material e.g. heparin. One of the benefits of having anticoagulant materials present on the surface of the device is that the device may thus be left in situ for several hours, during which time the blood/biological fluid conveying vessel can be repaired by a surgeon and the patient transported if necessary.

10 A modified device 201 according to a second embodiment of the present invention is shown in Fig. 5, in which like parts to the device in Figs. 1-4 are referenced by like reference numerals. The modified device 201 has a relatively narrow diameter waist portion 32 located between two relatively wide
15 diameter tubular end portions 34, 36 in the inflated state of the device. The inflated device thus has a substantially hour-glass profile, as shown in Fig. 5. In use of the device, the two end portions 34, 36 are located to either side of the damaged portion 6 of the blood vessel 4 so that the waist
20 section 32 is located at the damaged portion 6. With the device 201 inflated, the end portions 34, 36 provide a leak-proof seal between the device 201 and the inner wall of the blood vessel 4 thereby preventing blood leakage out of the vessel 4 at the damaged portion 6 thereof. This allows a
25 surgeon to repair the damaged portion 6 of the vessel 4. Furthermore, as a result of the relatively reduced diameter of the waist portion 32, an approximately annular space 38 is created between the inner (damaged) wall 30 of the blood vessel and the outer surface 28 of the waisted portion 32 of
30 the device. This annular space 38 allows a surgeon to work to repair the damaged portion 6 with a reduced risk of compromising the integrity of the device 201 by damage thereto by, for example, a surgical instrument (e.g. knife, needles or scissors) used by the surgeon during repair of the blood
35 vessel 4.

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A device 301 according to another modified embodiment of the present invention comprises a separately inflatable waist section 42 between first 44 and second 46 inflatable end portions, as shown in Fig. 6. The device 301 in a collapsed (non-inflated condition) is inserted into a blood vessel 4 to be repaired, and the first and second end portions 44, 46 are inflated by injecting saline into the inner volumes thereof. In this embodiment the central tube 20 incorporates two
10 separate channels in the thickness of the tube wall 25, one for delivering saline to the end portions 44, 46 and the other for delivering saline to the waist section 42. A first entry port 24 at the input end of the tube 20 is connected to a first one 50 of these two channels which feeds saline to one
15 or more support struts 22 which are in fluid communication with the first and second end portions 44 and 46 of the device. A second one 52 of these two channels connects a second entry port 26 in the tube 20 to the separately inflatable waist section 42, via a separate one of the support
20 struts 22.

Where the devices of Figs.1-6 are intended for use in occluding a damaged portion of the vena cava or hepatic veins, the length L of the inflatable tubular portion of the device
25 will typically be in the range of 13 to 17cm long, while the central tube 20 will typically be approximately 1 metre long. The diameter of the device, when collapsed, would typically be 3 to 4mm and, when inflated, about 2 to 2.5cm. However, it will be appreciated that the dimensions may be different for
30 where the device is intended for use in different blood vessels. E.g. for use in the aorta to, for example, occlude a diseased portion thereof, the inflatable tubular portion is likely to be approximately 7cm long and 4cm in diameter (when inflated).

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Figs. 7-9 illustrate a modified version of the device of Fig. 3, for achieving control of extravasation while preventing ischaemia (reduction in blood flow) to other body parts.

(Again, like parts to Figs. 1-4 are referenced by like reference numerals). This embodiment would be used for cases where a body part is supplied with blood via a blood vessel which branches off from the damaged blood vessel 4 (which may, for example, be a main blood vessel which is damaged or injured very close to, or at the branching point, from which the body part derives its blood supply). In a case like this, the normal placement of a device such as shown in Figs. 3, 5 or 6 may occlude the branching point of the vessel supplying the body part. This would occur if for example the inferior vena cava was damaged close to the hepatic or renal veins, or where there was an aneurysm 60 below the renal arteries 58, as shown in Fig.9. In either of these cases, if blood flow to these branching vessel(s) was interrupted for any significant period of time such as would be required to repair the damaged blood vessel, then the function and vitality of the liver and kidneys respectively would be considerably compromised, perhaps fatally so.

Thus according to the modified embodiment of Figs.7-9, the inflatable device 401 is provided with a relatively narrow neck portion 54 with openings 56 therein which allow blood flowing through the passage 8 in the device 401 (in use thereof) to enter from, or exit to, blood vessels 58 branching off from the main (damaged) blood vessel 4. As seen most clearly from Figs. 8, the openings 56 are positioned to allow blood to flow out of the passage 8, generally perpendicularly to normal blood flow through the passage 8. As explained above, this device 401 is particularly suitable for use when repairing a leaking aneurysm 60 (Fig. 9) while maintaining a blood supply to, for example the renal arteries 58. This is of significant benefit as the kidneys (or other organs) can

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thus be supplied with blood throughout the period in which the surgeon effects a repair to the main blood vessel 4, or where transfer of the patient to another location is required, or where there is any delay while an expert is in transit to the patient's location, thus controlling the leak and simultaneously allowing renal perfusion.

The relative positions of the openings 56 are chosen to suit the particular purpose i.e. the positions will generally be dependant upon which organs are to be maintained with a blood supply. Where only one organ is to be supplied, then a device 401 with only one opening may be used. As will be appreciated the blood supply required by various organs is different and so too is the vessel size supplying blood to the organ(s), therefore the openings may correspondingly be of different sizes to accommodate various blood flow requirements.

Figs 10 and 11 show a yet further modified embodiment of a device according to the present invention as indicated generally by the reference numeral 501. The device 501 is cylindrical, being equal diameter as it extends between first 62 and second 64 ends. The device 501 has an outer wall 66 which is in leak-proof contact with the intima 68 Fig 12 of the Inferior Vena Cava 70.

25

The device 501 has an oval shaped depression 72 (see shaded region in Fig 11) formed mid-way between the first and second ends 62, 64. The depression 72 has an outer edge 74 which is in leak-proof contact with the intima 68 when the device 501 is in an inflated condition. The depression 72 forms a working area for a surgeon to operate. As indicated in Fig 12, the device 501 when inserted into the IVC and locating the depression over the hepatic veins 76, allows a surgeon to incise about the hepatic veins to form a cuff 78 (Fig 13) and thereby effect removal of the liver 80. The device 501 as

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hereinbefore described is particularly useful in allowing a surgeon to form the cuff 78 during organ transplantations such as for the liver (Figs 12 and 13) and other organs such as the kidneys.

5

In a further preferred embodiment as shown in Figs 14A and 14B, the device 601 is formed from three inflatable semi-circular section wall portions 82a,b,c arranged to extend radially from the centre of the device 601. Each wall portion 10 82a,b,c has two major sides 84a,b which extend along the length of the device 601.

An inflatable strut 86a,b,c extends inwardly from an inner surface 88 of each of the walls 82a,b,c. Each strut 86a,b,c 15 is in fluid communication with the respective wall portion 82a,b,c at a first end 90a,b,c of each strut 86a,b,c, whereas all three struts 86a,b,c are also in fluid communication with one another at second ends 92a,b,c thereof where the struts 86a,b,c are conjoined to one another. In a deflated state as 20 shown in Fig 14A, the major edges 84a,b of the wall portions 82a,b,c are spaced apart from one another. When in an inflated state (Fig 14B) the major edges 84a,b of adjacent wall portions 84a,b,c are in full contact with one another so that fluid may pass through the device 601 without leakage 25 between the major edges 84a,b.

It will be appreciated that various modifications to the above-described embodiments are possible. For example, the guide wire may be formed from a so-called "memory" material 30 which material adopts a pre-determined shape or configuration where the device is in situ within the lumen of the damaged vessel, or other desired location.

Furthermore saline could be fed to the inflatable volume of 35 any of the above-described devices by a tube connected

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directly to the generally cylindrical (or hour-glass shaped) annular member of the device, instead of incorporating a saline channel in the wall of the central tube 20. In this case there may be no central tube 20 provided.

5

It will further be appreciated that as well as being applicable for use in control of extravasation from, for example, the IVC or hepatic veins, this being most commonly required in trauma cases, the above-described device is also
10 suitable for management of non-trauma diseases such as aortocava fistula (i.e. direct communication between aorta and IVC due to aneurysm etc), where the device could be used to retain blood flows in their respective lumina.

15 Furthermore, and as already mentioned above, the device may be used in the deployment of a stent in a blood vessel. The stent may simply be threaded over the inflatable tubular portion of the device 1 of Figs.1-4 above, for example, so that the stent is coaxial with and circumferentially surrounds the inflatable
20 device. The inflatable device is then inserted into the desired blood vessel in the same manner as described above, and then inflated so as to deploy the stent to its expanded state. Again, the advantage of blood being able to flow through the inflatable tubular portion of the device is that
25 normal or near normal blood flow is maintained in the patient while the stent is deployed to its expanded state in which it supports the blood vessel wall.

A further modification that may be made to the device of the
30 present invention, particularly where the device is to be used for a specific type of procedure is where the device is to be used for stenting, then the device may be provided with radiological markers thereon. To facilitate visualising the position and location of the device within a vessel (such as
35 the Aorta) during X-Ray screening, the balloon or inflatable

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tube portion may be provided with radiological markers at each end. Additionally or alternatively the radiological markers may be located or scaled so as to facilitate assessment of the internal diameter of the vessel.

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CLAIMS

1. An inflatable device for inserting, in a substantially
5 deflated state, into a blood or other biological fluid
carrying vessel of a human or animal, the device having an
inflated state in which it defines an elongate open-ended tube
means defining a passage means therethrough via which the
blood or other biological fluid in the vessel flows through
10 the device in use thereof.

2. A device as claimed in claim 1 wherein the elongate tube
means defined by the inflated device comprises an inlet end
and an outlet end and said passage means comprising at least
15 one passage, defined therebetween, through the longitudinal
length of the device.

3. A device as claimed in claim 1 wherein the form of the
device provides a close fit with the intima of the vessel in
20 use of the device.

4. A device as claimed in any one of claims 1 to 3 wherein
the diameter of said passage means is sufficiently large that
the blood or other biological fluid can flow relatively
25 unhindered through the device.

5. A device as claimed in claim 4 wherein the diameter of
said passage means is greater than 50% of the outer diameter
of the inflated device.

30

6. A device as claimed in claims 4 or 5 wherein the diameter
of said passage means is in the range of 90 to 95% of the
outer diameter of the inflated device.

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7. A device as claimed in any one of claims 1 to 6 wherein the device comprises one or more substantially collapsible walls defining a substantially enclosed inflatable volume which can be inflated by injecting saline or another
5 physiologically acceptable fluid, or combination of fluids, into the enclosed inflatable volume.
8. A device as claimed in any one of claims 1 to 7 wherein the device has a cross-section which is generally circular or
10 elliptical when inflated.
9. A device as claimed in any one of claims 1 to 7 wherein the device has an irregular cross-section when inflated, according to the particular shape or configuration of the
15 damaged blood or biological fluid carrying vessel in which the device is to be used.
10. A device as claimed in any one of claims 1 to 9 wherein in use of the device in a vessel having an injury area, the
20 device has a length which extends to at least the same length as said injury area in a said vessel.
11. A device as claimed in any one of claims 1 to 10 wherein the device has a working or conduit extending at least part-
25 way through the device wherein the working channel or conduit is formed and arranged for receiving therein at least one of the group comprising : a fluid, a device and a guide-wire.
12. A device as claimed in claim 11 wherein the working
30 channel or conduit is the hollow interior of an elongate conduit centrally positioned within the passage means.
13. A device as claimed in claim 12 wherein the elongate conduit is integrally formed with the inflatable device.

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14. A device as claimed in claims 12 or 13 wherein the elongate conduit is fixed to the device at at least one point therealong, with opposite end portions of the elongate conduit protruding from respective opposite ends of the tube means
5 defined by the inflated device.

15. A device as claimed in claims 12 to 14 wherein a first one of said protruding end portions is relatively long while the second end portion protrudes only a very short length
10 beyond the tube means forming the inflated device.

16. A device as claimed in claim 15 wherein said first protruding end portion is provided with a first self-sealing entry port to allow the admission of fluids materials or
15 devices, into the working channel, for delivery into a patient's bloodstream.

17. A device as claimed in any one of claims 1 to 16 wherein the device has attached thereto a guide wire to assist in the
20 insertion and positioning of the device.

18. A device as claimed in any one of claims 12 to 17 wherein a wall forming the elongate conduit contains, in the thickness thereof, a second channel which is in fluid communication with
25 the inflatable volume of the device, and through which a biologically compatible fluid is injected into the device in order to inflate the device.

19. A device as claimed in claim 18 wherein an input end of
30 the second channel terminates in and is connected to a second self-sealing entry port provided in the same end portion of the elongate conduit as the first entry port.

20. A device as claimed in claims 18 or 19 wherein one or
35 more walls forming central elongate conduit contain one or

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more further channels in fluid communication with further separate entry ports provided on the same protruding end of the central elongate conduit, for separately carrying one or more of a biologically compatible fluid, contrast imaging fluids and other fluids or devices therealong, to, from or through the device.

21. A device as claimed in any one of claims 1 to 20 wherein the device has at least one inflatable support strut within the passage means.

22. A device as claimed in claim 21 wherein the at least one strut spans the inner diameter of the device.

23. A device as claimed in either one of claims 21 and 22 wherein the at least one support strut has a hollow interior which is in fluid communication with the enclosed inflatable volume of the device.

24. A device as claimed in any one of claims 22 or 23 wherein two, three, four or more support struts are provided.

25. A device as claimed in any one of claims 21 to 24 when dependant on any one of claims 12 to 20 wherein the at least one support strut is formed and arranged such that, in the inflated state of the device, the strut extends radially outwardly from the central elongate conduit to an annular outer portion of the inflated device.

26. A device as claimed in any one of claims 21 to 25 when dependant on any one of claims 12 to 20 wherein the at least one support strut is in fluid communication with the inner channel formed in the wall of the central elongate conduit.

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27. A device as claimed in any one of claims 1 to 26 wherein the inflated device is non-uniform in outer diameter along the longitudinal length thereof.

5 28. A device as claimed in any one of claims 1 to 27 wherein the inflated device presents a generally hour-glass shaped side profile, having a relatively narrow waist portion and relatively wide end portions.

10 29. A device as claimed in claim 28 wherein the device in its inflated condition, provides a leak-proof fit with the intima of the blood/biological fluid conveying vessel and the waist portion defines a working space between the outer surface of the device and the intima of the blood/biological fluid
15 conveying vessel.

30. A device as claimed in either of claims 28 and 29 wherein the waist portion is separately inflatable from the rest of the inflatable volume of the device.

20

31. A device as claimed in any one of claims 2 to 30 wherein the device is provided with one or more openings which are formed and arranged to allow perfusion of blood therethrough from the passage means in a flow direction generally
25 perpendicular to the axis of the device when said opening are located at branching points with a branched vessel.

32. A device as claimed in claim 31 wherein the device has a non-uniform diameter along its length, having a relatively
30 narrow first end portion provided with said openings, and a relatively wide second portion.

33. A device as claimed in claims 27 to 32 wherein the device has a waist portion disposed between first and second ends of
35 the device, wherein the waist portion has a reduced outer

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diameter portion extending at least part-way around the outer circumference of the device and defines a working area between the intima of a said vessel and the inflated device.

5 34. A device as claimed in claim 33 wherein the reduced outer diameter portion has a longitudinal extent at least as great as its extent about the circumference of the device.

35. A device as claimed in any one of claims 21 to 34 where
10 the tube forming the device is formed from at least two inflatable semi-circular wall portions, each wall portion having two major longitudinally extending edges which extend substantially parallel to a corresponding edge of an adjacent wall portion; said at least two wall portions are in fluid
15 communication with a said support strut, wherein said support strut is formed and arranged to align the respective major edges of the at least two wall portions such that the major edges of adjacent wall portions abut against one another to form a more or less fluid tight seal therebetween and along
20 the extent thereof when the device is in an inflated condition.

36. A kit of parts comprising an inflatable device as claimed in any one of claims 1 to 35 for inserting into a
25 blood or other fluid carrying vessel, and insertion means for facilitating access to the inside of said vessel.

37. A kit-of-parts as claimed in claim 36 which includes deployment means for deploying the device to its inflated
30 condition.

38. A method of controlling extra-vascular haemorrhage comprising the steps of:
inserting an inflatable device of claim 1, in its deflated
35 condition, into a damaged blood vessel;

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locating the device adjacent to a damaged portion of the blood vessel; and

inflating the device so as to substantially occlude the damaged portion so as to minimise leakage of blood from said
5 damaged portion.

39. A method of inserting and deploying a stent in a blood vessel comprising the steps of:

10 locating an expandable generally tubular stent, in a collapsed state thereof, of the device of claim 1 so that the stent is coaxial with and circumferentially surrounds the inflatable device;

inserting the inflatable device, in its deflated condition, and with the stent located thereon, into a blood vessel to be
15 stented and locating the device in the desired portion thereof; and

inflating the device so as to deploy the stent to an expanded condition in which it supports the wall of the blood vessel.

20 40. A device as claimed in any one of claims 1 to 39 wherein the device is fabricated from one or more physiologically acceptable materials selected from the group including rubber, synthetic rubber, and plastics materials, polyurethane, polyethylene, Pluronic (RTM), and/or block, and/or co-polymers
25 thereof.

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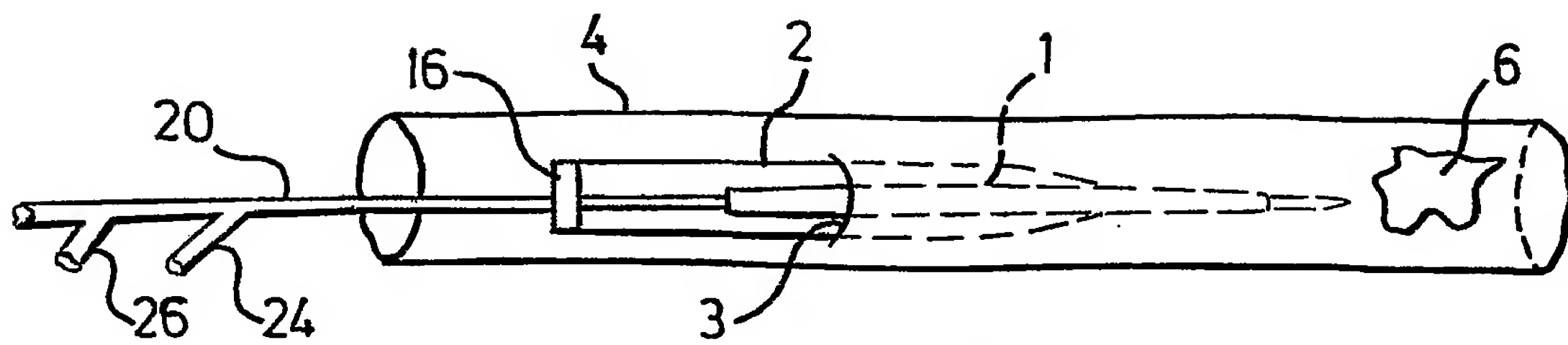


Fig.1

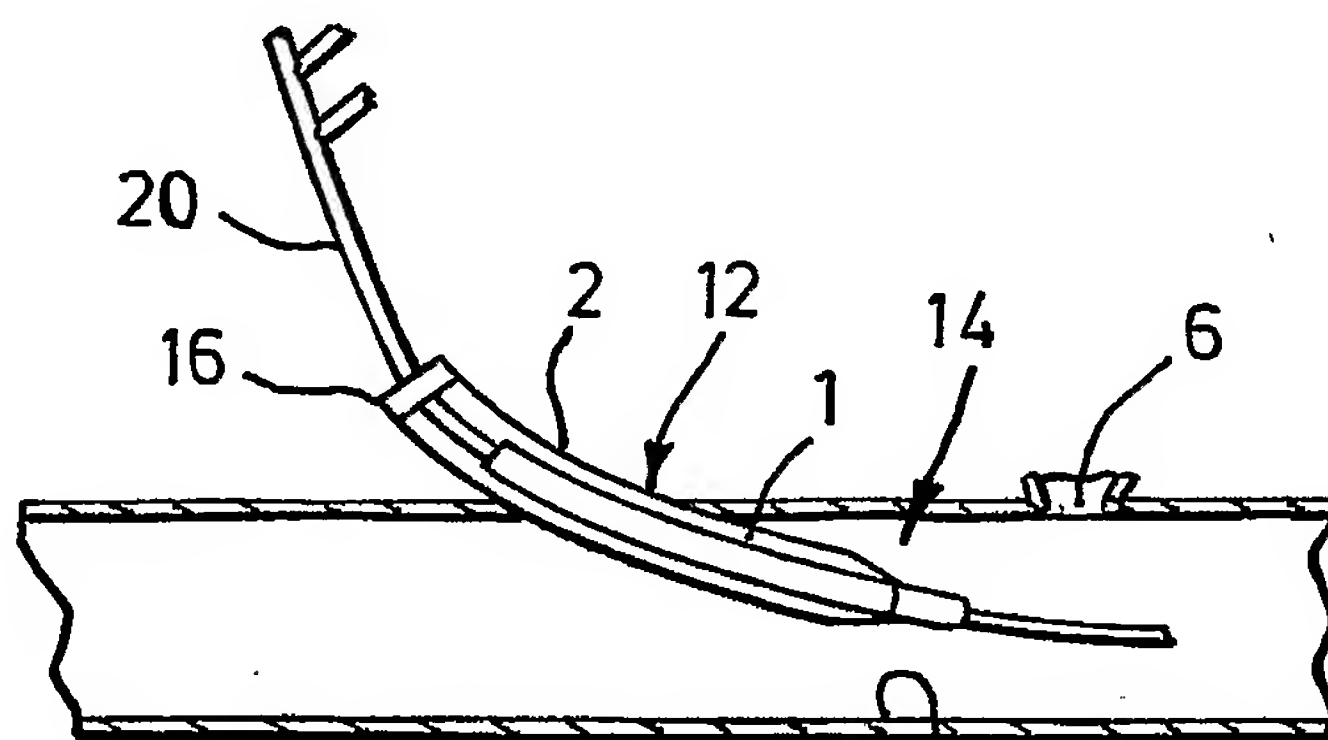


Fig.2

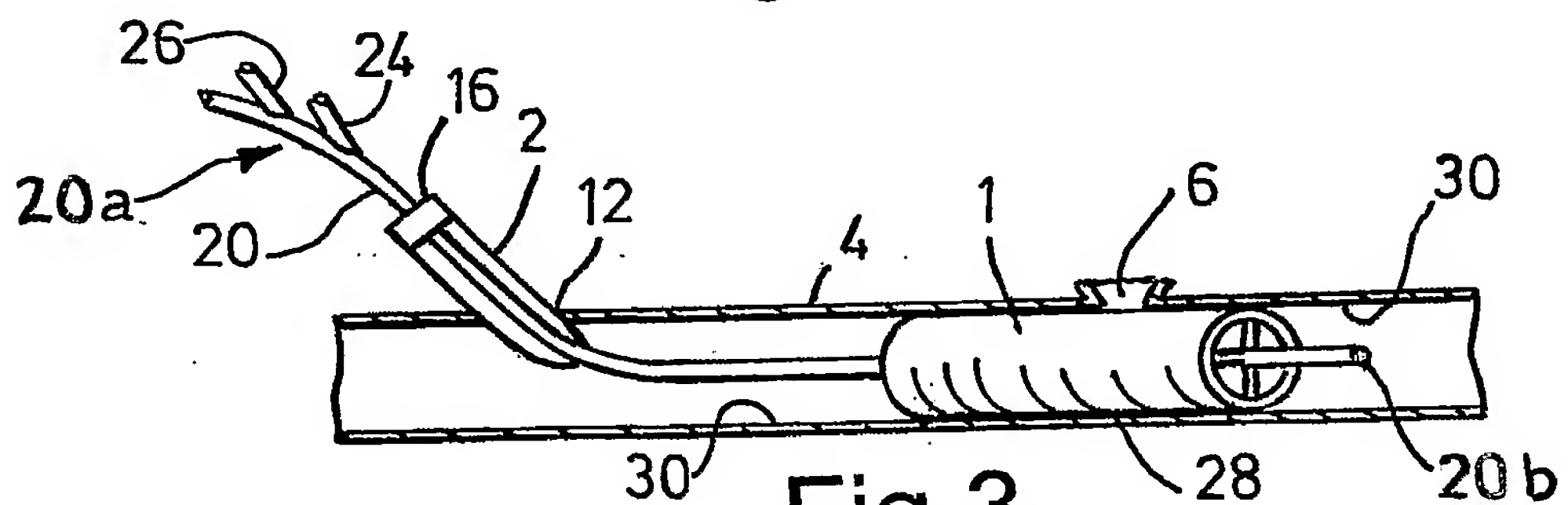


Fig.3

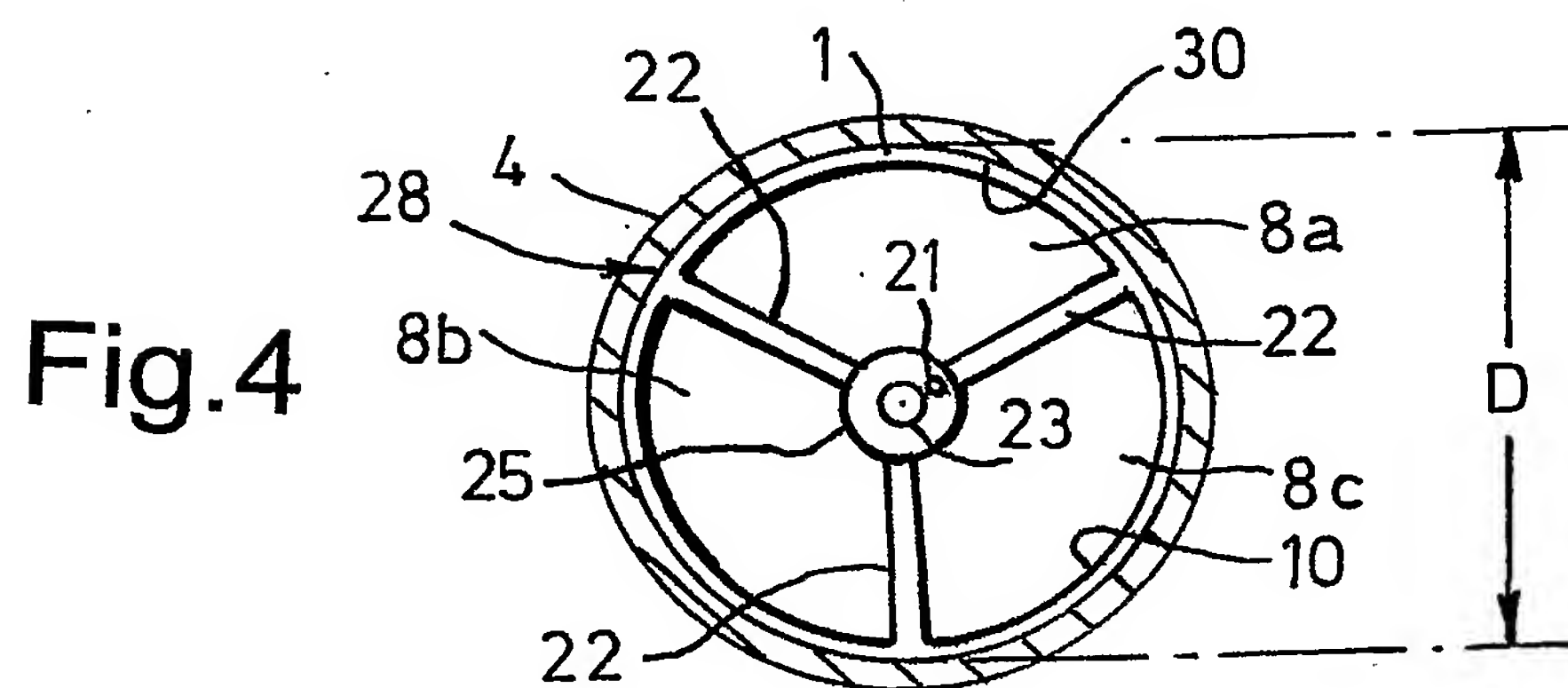


Fig.4

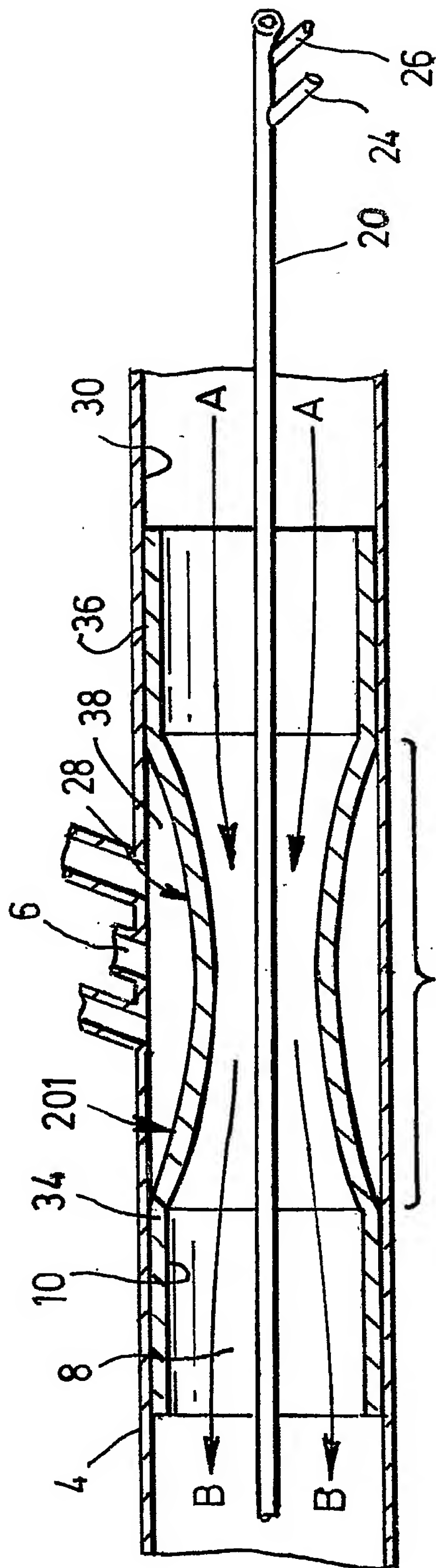


Fig. 5

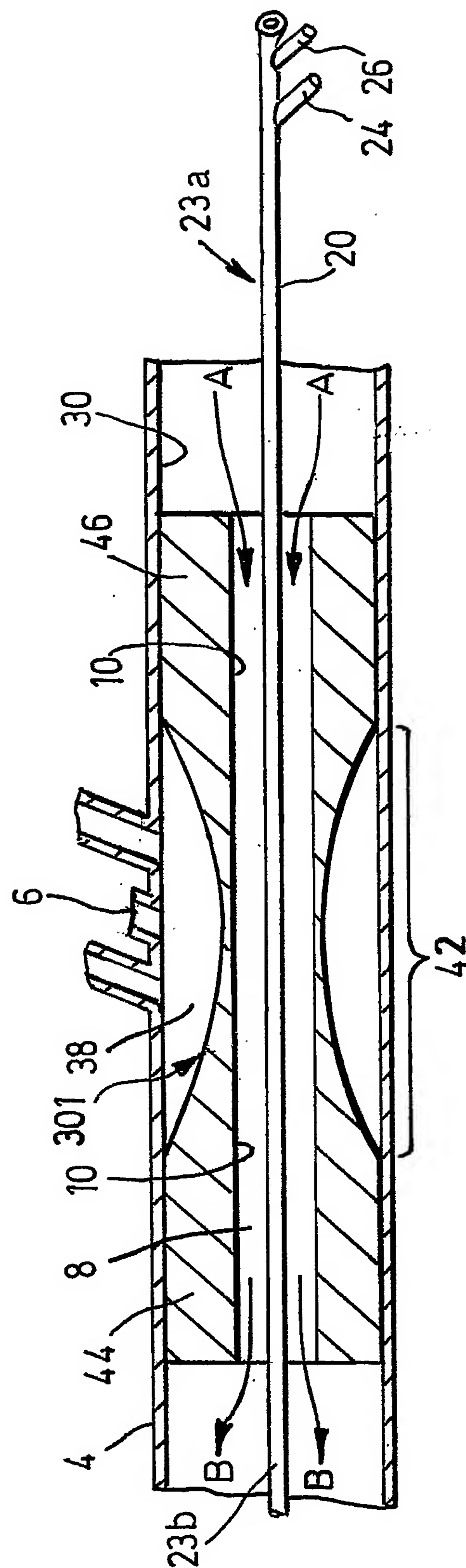


Fig. 6

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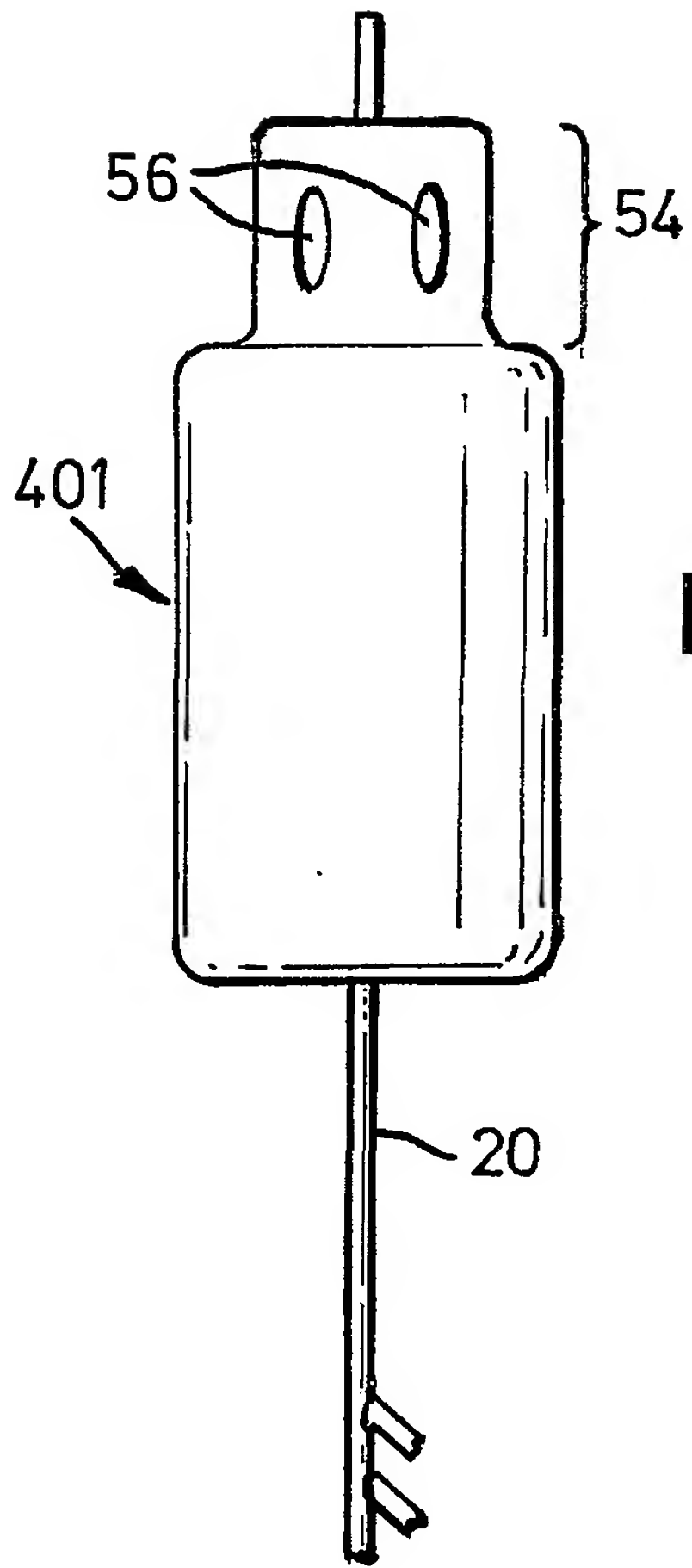


Fig.7

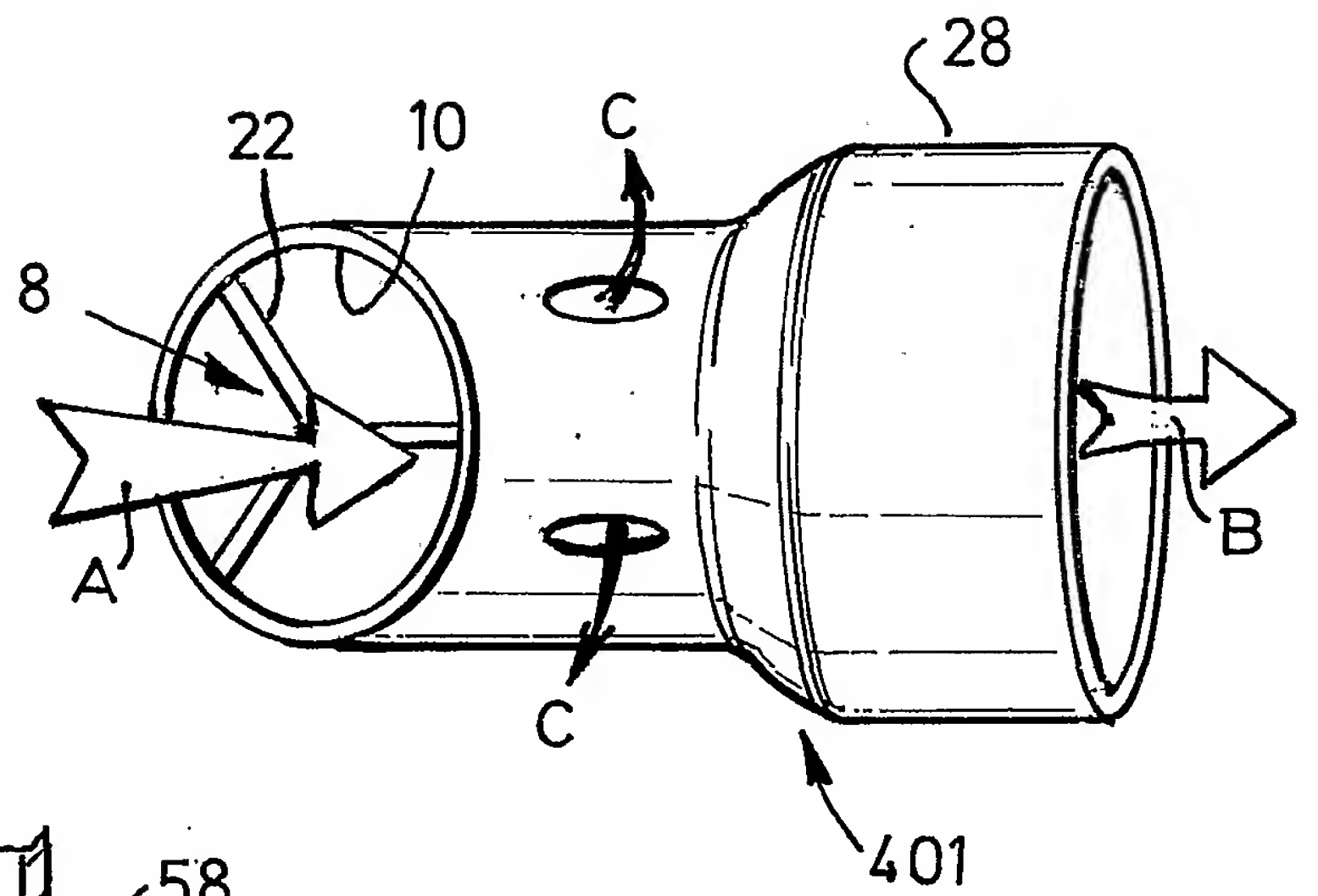


Fig.8

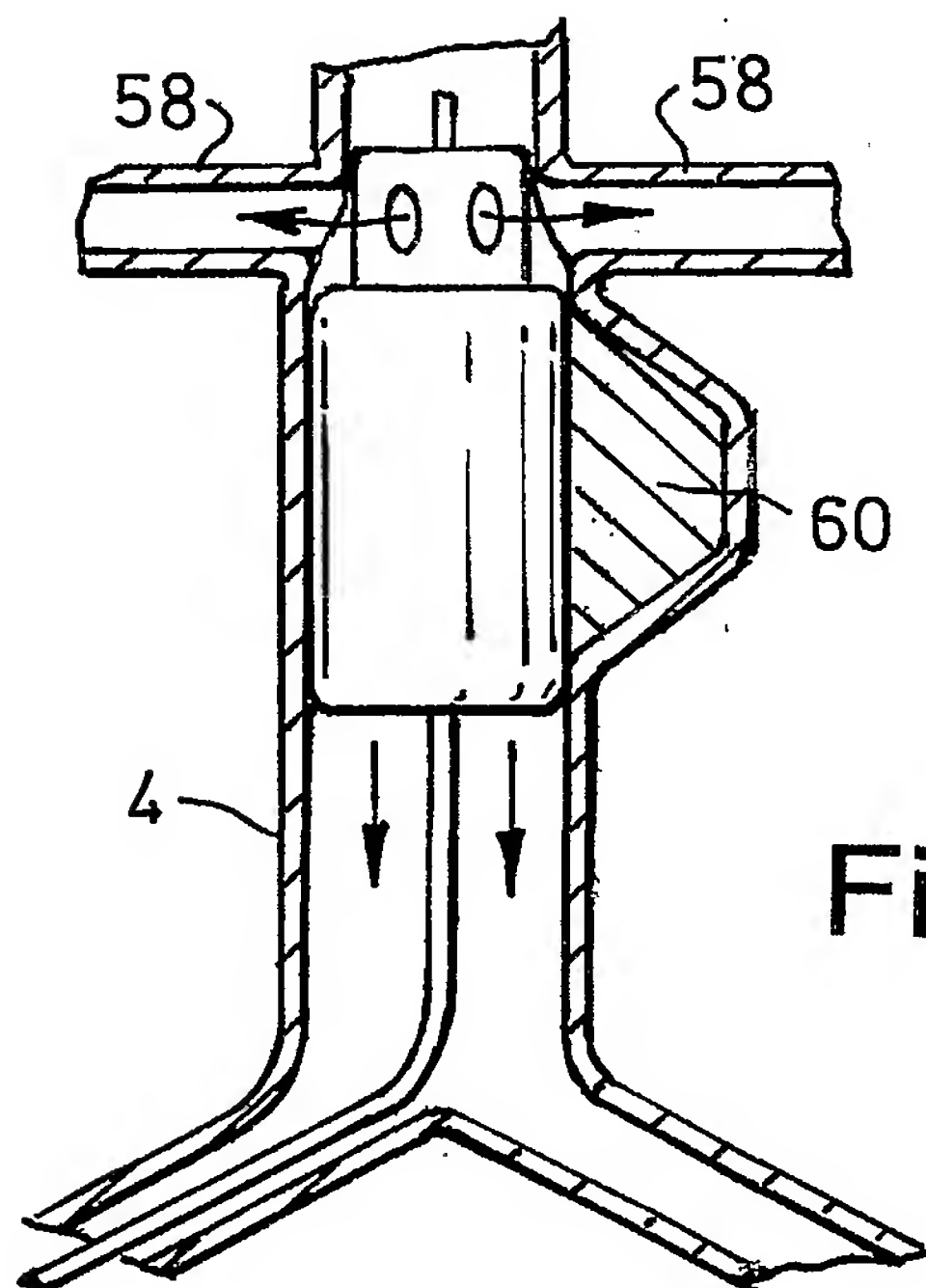


Fig.9

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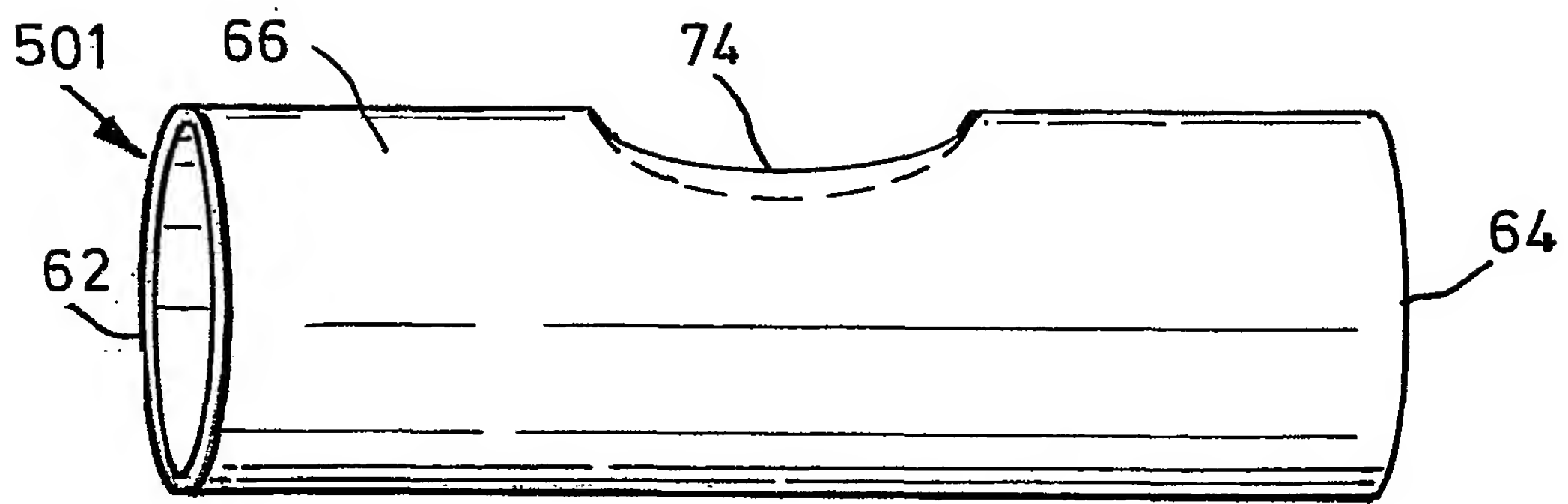


Fig.10

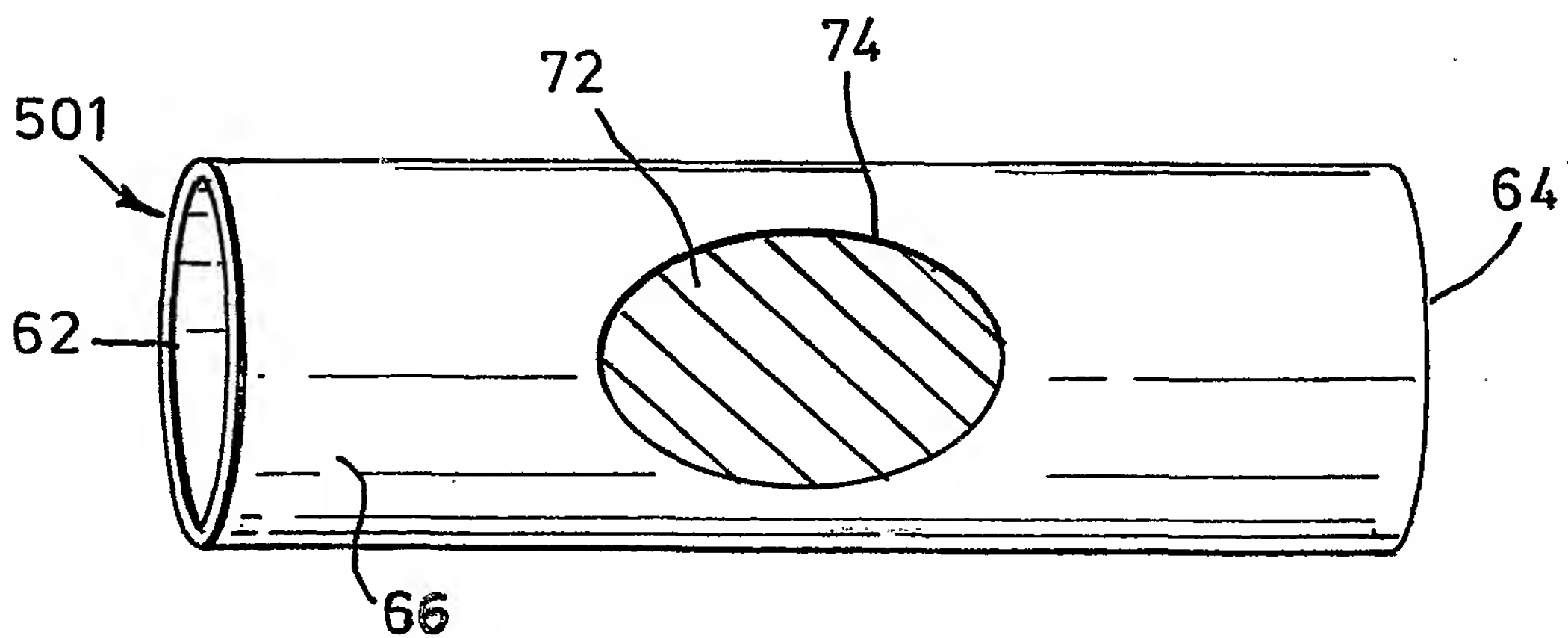


Fig.11

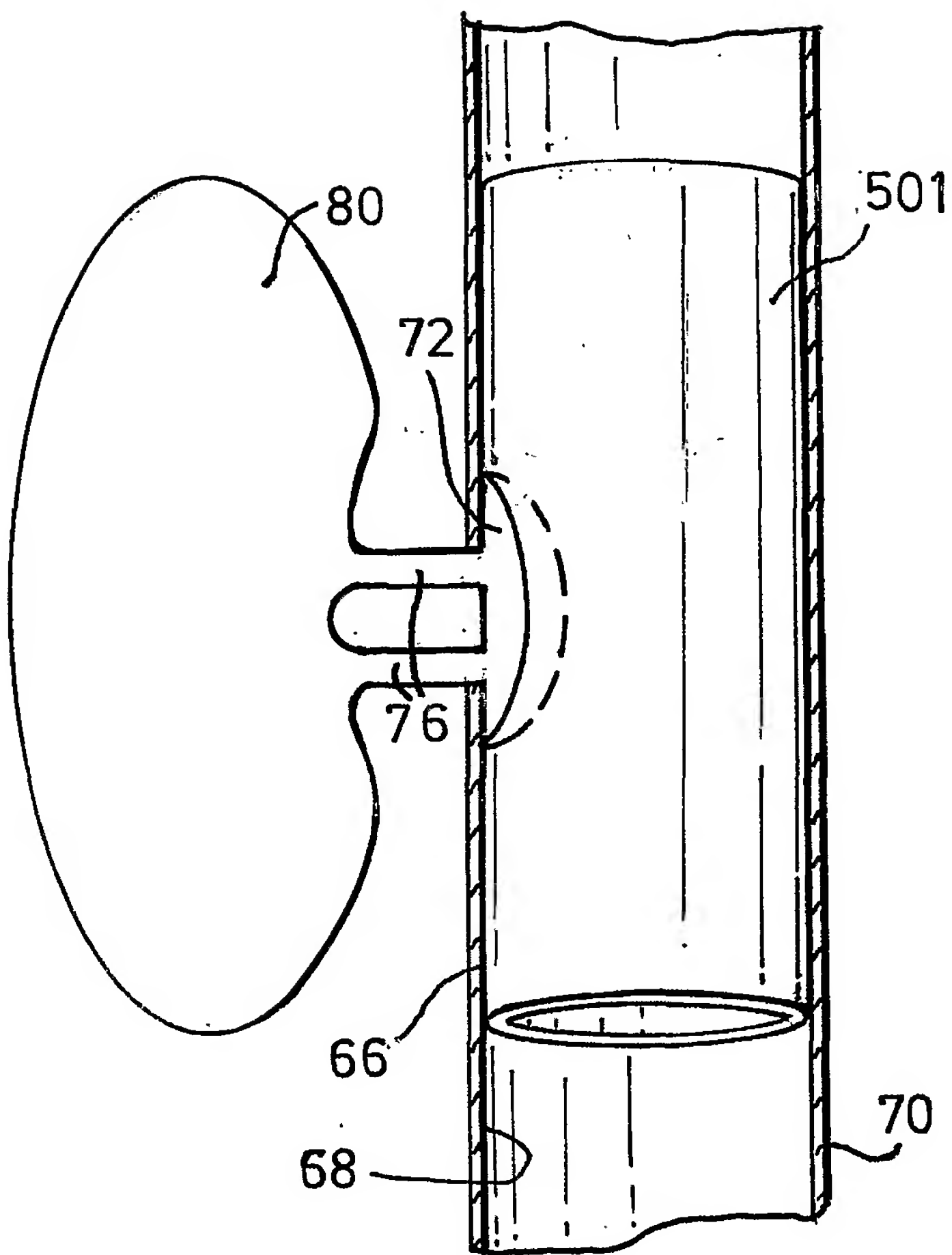


Fig.12

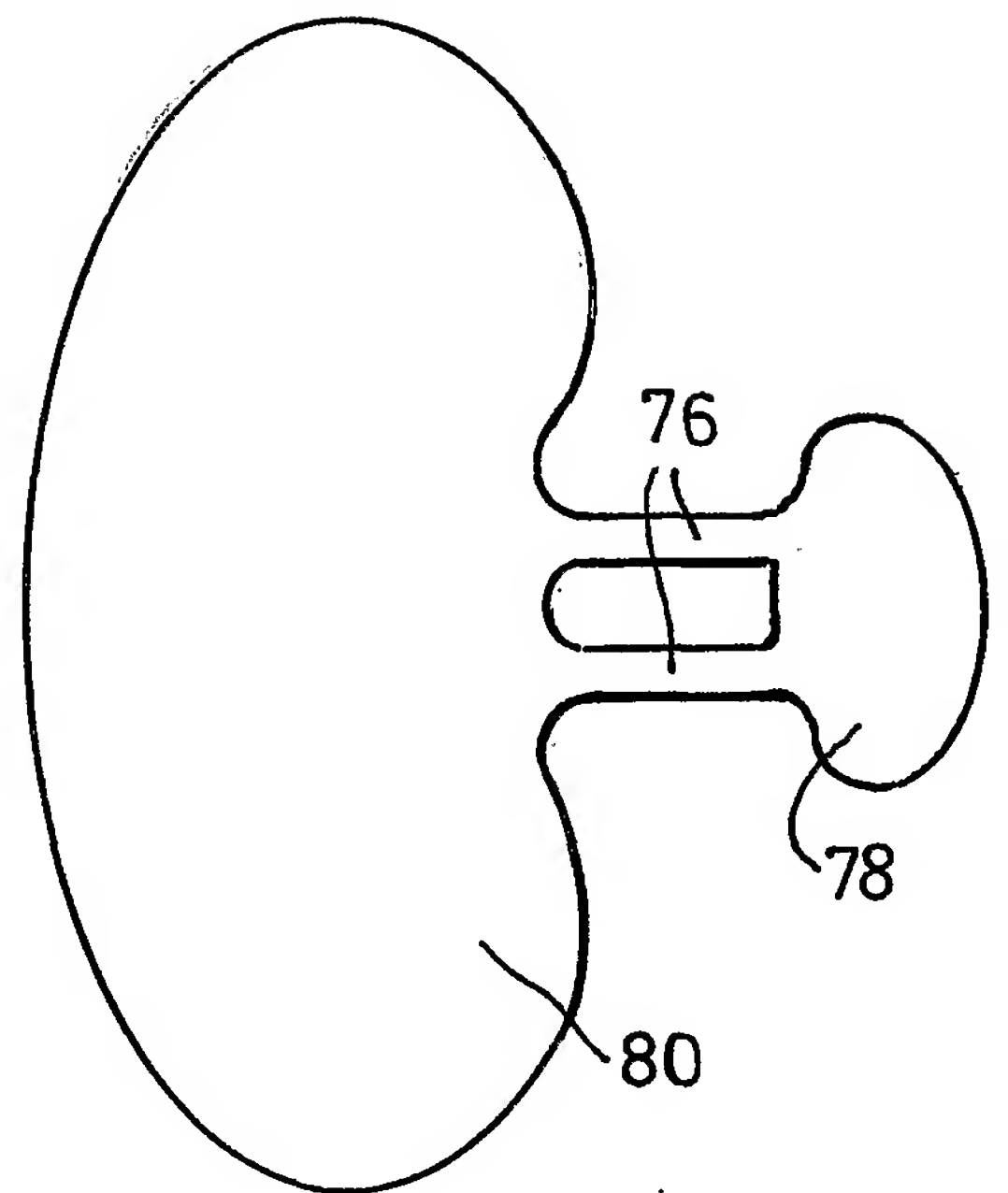


Fig.13

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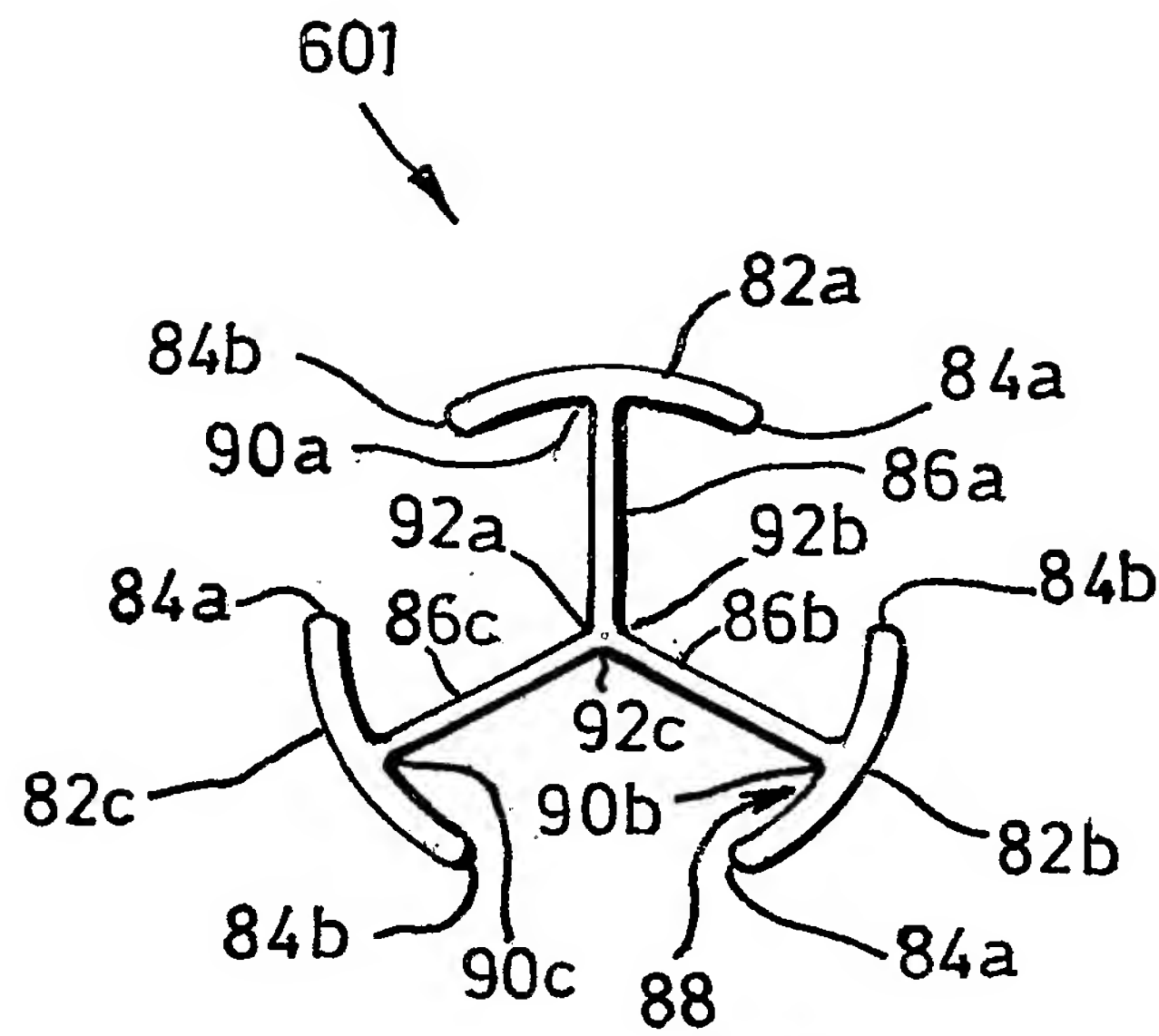


Fig.14A

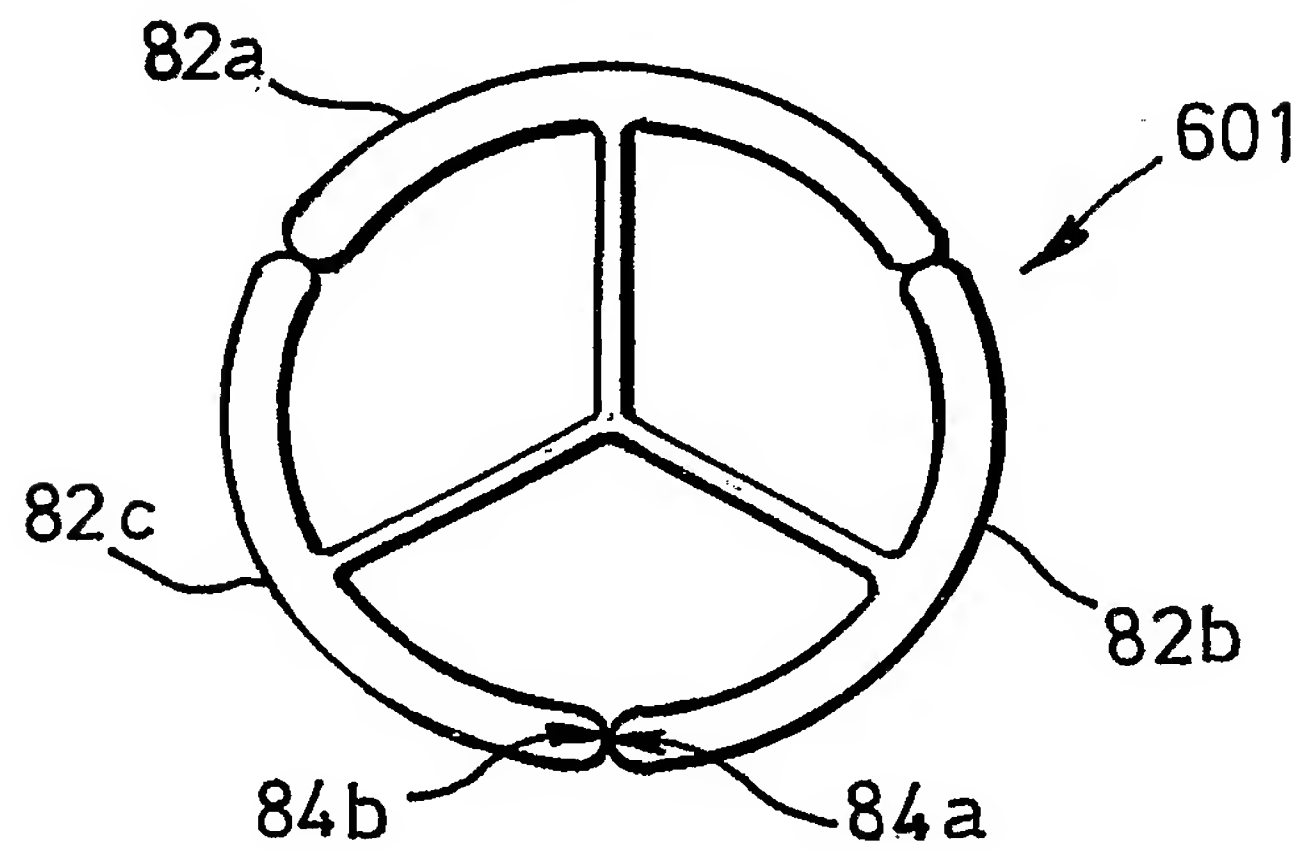


Fig.14B

INTERNATIONAL SEARCH REPORT

International Application No

PCT/GB 00/04877

A. CLASSIFICATION OF SUBJECT MATTER
 IPC 7 A61M29/00 A61M25/00 A61B17/12 A61F2/06

According to International Patent Classification (IPC) or to both national classification and IPC

B. FIELDS SEARCHED

Minimum documentation searched (classification system followed by classification symbols)

IPC 7 A61M A61B A61F

Documentation searched other than minimum documentation to the extent that such documents are included in the fields searched

Electronic data base consulted during the international search (name of data base and, where practical, search terms used)

EPO-Internal

C. DOCUMENTS CONSIDERED TO BE RELEVANT

Category *	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
X	US 5 954 741 A (FOX ROGER HARRINGTON) 21 September 1999 (1999-09-21) column 3, line 25 -column 4, line 36; figures 2-6 ---	1-23
X	WO 97 40889 A (APPLE MARC G ;APPLE MELVIN J (US)) 6 November 1997 (1997-11-06) the whole document ---	1-36
X	WO 95 05860 A (BOSTON SCIENT CORP) 2 March 1995 (1995-03-02) page 6, line 28 -page 7, line 30; figure 2 ---	1
A	US 5 397 307 A (GOODIN RICHARD) 14 March 1995 (1995-03-14) column 4, line 41 -column 6, line 55; figure 1 --- -/--	33

☒ Further documents are listed in the continuation of box C.

☒ Patent family members are listed in annex.

* Special categories of cited documents :

"A" document defining the general state of the art which is not considered to be of particular relevance
 "E" earlier document but published on or after the international filing date
 "L" document which may throw doubts on priority claim(s) or which is cited to establish the publication date of another citation or other special reason (as specified)
 "O" document referring to an oral disclosure, use, exhibition or other means
 "P" document published prior to the international filing date but later than the priority date claimed

"T" later document published after the international filing date or priority date and not in conflict with the application but cited to understand the principle or theory underlying the invention
 "X" document of particular relevance; the claimed invention cannot be considered novel or cannot be considered to involve an inventive step when the document is taken alone
 "Y" document of particular relevance; the claimed invention cannot be considered to involve an inventive step when the document is combined with one or more other such documents, such combination being obvious to a person skilled in the art.
 "&" document member of the same patent family

Date of the actual completion of the international search

27 March 2001

Date of mailing of the international search report

04.04.01

Name and mailing address of the ISA

European Patent Office, P.B. 5818 Patentlaan 2
 NL - 2280 HV Rijswijk
 Tel. (+31-70) 340-2040, Tx. 31 651 epo nl,
 Fax: (+31-70) 340-3016

Authorized officer

Ehrsam, F

INTERNATIONAL SEARCH REPORT

International Application No

PCT/GB 00/04877

C.(Continuation) DOCUMENTS CONSIDERED TO BE RELEVANT

Category °	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
A	US 5 843 116 A (CROCKER MICHAEL ET AL) 1 December 1998 (1998-12-01) column 17, line 10 -column 22, line 65; figures 10-18 ---	21-32
A	WO 99 20324 A (BERSIN ROBERT D) 29 April 1999 (1999-04-29) the whole document ---	1
A	US 4 832 688 A (SAGAE KYUTA ET AL) 23 May 1989 (1989-05-23) figures 5A-5I ---	1-3
A	GB 1 538 737 A (MEDICAL ENG CORP) 24 January 1979 (1979-01-24) claims 1-3; figures 3A-3C -----	35

INTERNATIONAL SEARCH REPORT

national application No.
PCT/GB 00/04877

Box I Observations where certain claims were found unsearchable (Continuation of item 1 of first sheet)

This International Search Report has not been established in respect of certain claims under Article 17(2)(a) for the following reasons:

1. ☒ Claims Nos.: **38-40**
because they relate to subject matter not required to be searched by this Authority, namely:
A meaningful search is not possible on the basis of all claims because all claims are directed to - Method for treatment of the human or animal body by surgery - Rule 39.1(iv) PCT
2. ☐ Claims Nos.:
because they relate to parts of the International Application that do not comply with the prescribed requirements to such an extent that no meaningful International Search can be carried out, specifically:
3. ☐ Claims Nos.:
because they are dependent claims and are not drafted in accordance with the second and third sentences of Rule 6.4(a).

Box II Observations where unity of invention is lacking (Continuation of item 2 of first sheet)

This International Searching Authority found multiple inventions in this International application, as follows:

1. ☐ As all required additional search fees were timely paid by the applicant, this International Search Report covers all searchable claims.
2. ☐ As all searchable claims could be searched without effort justifying an additional fee, this Authority did not invite payment of any additional fee.
3. ☐ As only some of the required additional search fees were timely paid by the applicant, this International Search Report covers only those claims for which fees were paid, specifically claims Nos.:
4. ☐ No required additional search fees were timely paid by the applicant. Consequently, this International Search Report is restricted to the invention first mentioned in the claims; it is covered by claims Nos.:

Remark on Protest

- ☐ The additional search fees were accompanied by the applicant's protest.
- ☐ No protest accompanied the payment of additional search fees.

INTERNATIONAL SEARCH REPORT

Information on patent family members

International Application No

PCT/GB 00/04877

Patent document cited in search report		Publication date	Patent family member(s)	Publication date
US 5954741	A	21-09-1999	GB 2290236 A	20-12-1995
			AT 190853 T	15-04-2000
			AU 694237 B	16-07-1998
			AU 2680095 A	05-01-1996
			CA 2192978 A	21-12-1995
			DE 69515874 D	27-04-2000
			DE 69515874 T	07-12-2000
			EP 0766574 A	09-04-1997
			WO 9534339 A	21-12-1995

WO 9740889	A	06-11-1997	US 5916143 A	29-06-1999
			AU 2993797 A	19-11-1997
			CA 2252475 A	06-11-1997
			EP 0959948 A	01-12-1999
			US 6117064 A	12-09-2000

WO 9505860	A	02-03-1995	CA 2170157 A	02-03-1995
			EP 0746362 A	11-12-1996
			JP 9501598 T	18-02-1997
			US 5693014 A	02-12-1997
			US 5746745 A	05-05-1998
			US 6010480 A	04-01-2000

US 5397307	A	14-03-1995	AT 176761 T	15-03-1999
			AU 682896 B	23-10-1997
			AU 7791494 A	27-06-1995
			CA 2176753 A	15-06-1995
			DE 69416603 D	25-03-1999
			DE 69416603 T	09-09-1999
			EP 0732958 A	25-09-1996
			WO 9515782 A	15-06-1995
			JP 2874800 B	24-03-1999
			JP 9500312 T	14-01-1997

US 5843116	A	01-12-1998	US 6027486 A	22-02-2000
			US 5645560 A	08-07-1997
			AU 2930897 A	19-11-1997
			EP 0904124 A	31-03-1999
			JP 2000509304 T	25-07-2000
			WO 9740877 A	06-11-1997
			US 6120523 A	19-09-2000
			US 6027517 A	22-02-2000

WO 9920324	A	29-04-1999	AU 1190699 A	10-05-1999

US 4832688	A	23-05-1989	JP 1924425 C	25-04-1995
			JP 5022551 B	29-03-1993
			JP 62236560 A	16-10-1987
			EP 0241038 A	14-10-1987

GB 1538737	A	24-01-1979	DE 2713958 A	20-10-1977
			JP 52128681 A	28-10-1977
